**A Comparison between windowing FIR Filters for Extracting the EEG Components**

Elwathiq A. Mahmoud1, Abdalla H. Abdalla1, Ahmed M. Wedaa1, Mawia A. Hassan\*1,2

1Medical Engineering Department, University of Science & Technology, Omdurman, Sudan

2Biomedical Engineering Department, Sudan University of Science & Technology, Khartoum, Sudan

mawiaahmed@sustech.edu

*Abstract*

Electroencephalogram (EEG) is a test used to detect abnormalities related to electrical activity of the brain. In this work different finite impulse response filter (FIR) windows methods were used to extract EEG signal to its basic components (Delta wave, Theta wave, Alpha wave and Beta wave). The comparison between these windowing methods were done by computing the Fourier transform, power spectrum, SNR, the main-lobe, and the side-lobe. The results show the best main-lobe is for rectangular window, the best side-lobe is for Kaiser β (12) and the best SNR is for Hanning. Also the best window according to main-lobe, side-lobe and SNR is Kaiser β (12).

***Keywords***

*EEG, FIR, SNR, main-lobe, side-lobe.*

# INTRODUCTION

Electroencephalogram (EEG) used to measure abnormalities in the brain, which related to electrical activity (Fig.1). This measurement tracks and records brain wave patterns by using electrodes are placed on the scalp, and then signals go to a computer to record the results. Abnormal patterns in EEG indicate seizures and other problems [3][6]. The important reason for using EEG is to diagnose and show seizure disorders. Also EEGs help to help to identify causes of other problems like sleep disorders and changes in behavior. To evaluate the brain activity after head injury, or before heart or liver transplantation the EEG is a good choice [3]. The electrodes in the conventional scalp EEG are placed on the scalp with a conductive gel or paste which is led to reduce impedance due to dead skin cells. When used on high-density arrays of electrodes are needed many systems use caps or nets which electrodes are embedded in it. The Electrodes locations and names depend on an international 10–20 system for most clinical and research applications (except when high-density arrays are used). About 19 recording electrodes (plus ground and system reference) are used in most clinical applications. If the spatial resolution is the aim of interest further electrodes can be added for a particular area of the brain and this in clinical or research application. Up to 256 electrodes can be used in High-density arrays, it may become more-or-less evenly spaced around the scalp. Differential amplifier can be used to connect the electrode (one amplifier per pair of electrodes). The other input of each differential amplifier is connected by a common reference electrode. The job of these amplifiers is to amplify the voltage between the reference and active electrode and (1,000–100,000 times, or 60–100 dB voltage gain). Most EEGs systems nowadays are digital, the signal is amplified and pass through ADC and anti-aliasing filter. The sampling rate between 256–512 Hz in the clinical scalp EEG; in some research applications, it may use sampling rates of up to 20 kHz. For adult EEG signal is about 10 μV to 100 μV when the measuring from the scalp and is about 10–20 mV when measuring from subdural electrodes [4][3]. The fundamental components of the EEG system is shown in fig.1

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| Surface electrode  Pre- amplifier  Band –Reject filter  Isolation circuit  Band pass filter  Amplifier |
| FIG.1 EEG BLOCK DIAGRAM |

The basic signals in the EEG are: Delta wave with a frequency range up to 4 Hz. This wave is the highest in amplitude and the slowest waves [4]m theta wave has the frequency range from 4 Hz to 7 Hz. Theta is seen normally in young children[4][8], Alpha wave is the frequency range from 7 Hz to 14 Hz. Beta wave is the frequency range from 15 Hz to about 30 Hz. In areas of cortical damage this wave may may be reduced or absent. It is the dominant rhythm in patients who are alert or anxious or who have their eyes open [4][11].

One of the most basic elements in a digital signal processing system is The finite impulse response (FIR) filter. It can guarantee a linear phase frequency characteristic with frequency characteristic. Also the unit impulse response is finite. In this work different finite impulse response filter (FIR) windows methods were used to extract the EEG signal to its basic components (Delta wave, Theta wave, Alpha wave and Beta wave).

# METHODS

In this work comparison between different FIR windowing filters to extract EEG signal to its basic components (delta, theta, alpha and beta). The steps are:

1. EEG signals (Delta, theta, alpha and beta) were extracted by band-pass filter using Rectangular, Hamming, Hanning, Kaiser and Blackman windows (Table 1).

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| Table 1 Windowing functions | |
| **Window** | **Equation** |
| Rectangular | Y[n] = |
| Hamming | R[N] = |
| Kaiser | W [n] = |
| Hanning | W[n]= |
| Blackman | W[n]= |

1. The length of each window was calculated using equation 1. (Table 2).

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| /L-1 | 1 |

Where is the frequency resolution, G is the window factor, is the sampling frequency and L is the window length.

1. Compute the Fourier transform of each wave after extraction.
2. Compute the original power spectrum.
3. Compute the SNR for all signals.

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| FIG.2 COMPARISON BETWEEN EXTRACTED DELTA WAVE, (A) EEG SIGNAL, (B) USING RECTANGULAR, (C) USING HAMMING, (D) USING HANNING , (E) USING KAISER Β= 5, (F) USING KAISER Β= 8,(G) USING KAISER Β= 12, (H) USING BLACKMAN. | |

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| FIG.3 COMPARISON BETWEEN EXTRACTED THETA WAVE, (A) EEG SIGNAL, (B) USING RECTANGULAR, (C) USING HAMMING, (D) USING HANNING , (E) USING KAISER Β= 5, (F) USING KAISER Β= 8,(G) USING KAISER Β= 12, (H) USING BLACKMAN. | |

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| FIG.4 COMPARISON BETWEEN EXTRACTED ALPHA WAVE, (A) EEG SIGNAL, (B) USING RECTANGULAR, (C) USING HAMMING, (D) USING HANNING , (E) USING KAISER Β= 5, (F) USING KAISER Β= 8,(G) USING KAISER Β= 12, (H) USING BLACKMAN. | |

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| FIG.5 COMPARISON BETWEEN EXTRACTED BETA WAVE, (A) EEG SIGNAL, (B) USING RECTANGULAR, (C) USING HAMMING, (D) USING HANNING , (E) USING KAISER Β= 5, (F) USING KAISER Β= 8,(G) USING KAISER Β= 12, (H) USING BLACKMAN. | |

# RESULTS AND DISCUSSIONS

Table 2 is shown the length of each FIR window using equation 1.

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| Table2 the length of each FIR window | | | | | |
| Windows | | Signals | | | |
| Delta | Theta | Alpha | Beta |
| Rectangular | | 57 | 49 | 39 | 11 |
| Hamming | | 115 | 99 | 79 | 23 |
| Hanning | | 115 | 99 | 79 | 23 |
| Kaiser β | 5  8  12 | 114.2 | 100 | 79 | 23 |
| 171 | 149 | 119 | 35 |
| 227 | 199 | 159 | 47 |
| Blackman | | 171 | 149 | 119 | 35 |

Fig. 2, 3, 4, and 5 show the comparisons between the extracted the basic EEG components using rectangular, Hamming, Hanning, Kaiser (5, 8 and12) and Blackman.

Table 3 show the comparison between main-lobes, side-lobes and SNR for delta signal filtered by windowing method.

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| Table I main-lobes, side-lobes and SNR ratio for delta signal | | | |
| Window | Main-lobe -3 dB | Side-lobe dB | SNR dB |
| Rectangular | 0.0059 | -13.3 | -55.49 |
| Hamming | 0.0044 | -42.7 | -55.03 |
| Hanning | 0.0049 | -31.5 | -139.74 |
| Kaiser beta 5 | 0.0044 | -36.8 | -55.73 |
| Kaiser beta 8 | 0.0037 | -58.6 | -63.90 |
| Kaiser beta 12 | 0.0033 | -89.9 | -66.69 |
| Blackman | 0.0037 | -58.1 | -67.47 |

Table 4 show the comparison between main-lobes, side-lobes and SNR for theta signal filtered by windowing method.

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| Table4 main-lobes, side-lobes and SNR ratio for theta signal | | | |
| Window | Main-lobe -3 dB | Side-lobe dB | SNR dB |
| Rectangular | 0.0068 | -13.3 | -97.51 |
| Hamming | 0.0048 | -42.7 | -122.64 |
| Hanning | 0.0054 | -31.5 | -122.59 |
| Kaiser beta 5 | 0.0049 | -36.8 | -122.59 |
| Kaiser beta 8 | 0.0042 | -58.6 | -122.94 |
| Kaiser beta 12 | 0.0037 | -83.9 | -123.09 |
| Blackman | 0.0042 | -58.1 | -121.76 |

Table 5 show the comparison between main-lobes, side-lobes and SNR for alpha signal filtered by windowing method

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| Table5 main-lobes, side-lobes and SNR for alpha signal | | | |
| Window | Main-lobe -3 dB | Side-lobe dB | SNR dB |
| Rectangular | 0.0088 | -13.3 | -55.49 |
| Hamming | 0.0063 | -42.7 | -139.74 |
| Hanning | 0.0068 | -31.5 | -139.74 |
| Kaiser beta 5 | 0.0063 | -36.8 | -139.70 |
| Kaiser beta 8 | 0.0051 | -58.6 | -139.23 |
| Kaiser beta 12 | 0.0046 | -90.0 | -139.41 |
| Blackman | 0.0034 | -58.1 | -67.47 |

Table 6 show the comparison between main-lobes, side-lobes and SNR for beta signal filtered by windowing method.

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| Table6 main-lobes, side-lobes and SNR ratio for beta signal | | | |
| **Window** | **Main-lobe -3 dB** | **Side-lobe dB** | **SNR dB** |
| Rectangular | 0.0273 | -13.3 | -115.80 |
| Hamming | 0.0215 | -42.6 | -142.01 |
| Hanning | 0.0239 | -31.5 | -141.96 |
| Kaiser beta 5 | 0.0219 | -37.0 | -141.93 |
| Kaiser beta 8 | 0.0176 | -58.5 | -141.49 |
| Kaiser beta 12 | 0.0156 | -90.2 | -141.39 |
| Blackman | 0.0186 | -58.1 | -133.32 |

As can be shown best main-lobe is for rectangular window, the best side-lobe is for Kaiser β (12) and the best SNR is for Hanning. Also the best window according to main-lobe, side-lobe and SNR is Kaiser β (12).

# CONCLUSION

In this study a comparisons between rectangular, Hamming, Hanning, Kaiser (5, 8 and12) and Blackman to extracted the EEG signal were shown. The results shown the best main-lobe is for rectangular window, the best side-lobe is for Kaiser β (12) and the best SNR is for Hanning. Also the best window according to main-lobe, side-lobe and SNR is Kaiser β (12).

# REFERENCES

1. T. Scarabino and U. Salvolini, Atlas Of Morphology And Functional Anatomy Of The Brain, Naples-Italy, 2006.
2. Su Peng ,”Design and analysis of FIR filters based on Matlab” Electrical Engineering, Linnaeus University,2013.
3. <http://kidshealth.org./>
4. John j.webster, Medical Instrumentation Application and Design, 4th Edition, wiley, 2010
5. Steven w .smith, the scientist and enginreer’s ,guide to digital signal processing ,California technical publishing, 1999.
6. Niedermeyer E., [Ernst Niedermeyer](http://www.amazon.com/s/ref=dp_byline_sr_ebooks_2?ie=UTF8&field-author=Ernst+Niedermeyer&search-alias=digital-text&text=Ernst+Niedermeyer&sort=relevancerank) and [F. L. da Silva](http://www.amazon.com/s/ref=dp_byline_sr_ebooks_3?ie=UTF8&field-author=Fernando+Lopes+da+Silva+MD++PhD&search-alias=digital-text&text=Fernando+Lopes+da+Silva+MD++PhD&sort=relevancerank) ,Electroencephalography: Basic Principles, Clinical Applications, and Related Fields, Lippincot Williams & Wilkins, 2004.
7. Towle, Vernon L, Bolaños. José; Suarez. Diane and Levin. David N, “The spatial location of EEG electrodes Locating the best-fitting sphere relative to cortical anatomy", Electroencephalography and Clinical Neurophysiology, vol.86, no. 1, pp. 1-6 ,1993.
8. Cahn, B. Rael and Polich John, “Meditation states and traits: EEG, ERP, and neuroimaging studies”, Psychological Bulletin, vol.132, no. 2, pp. 180-211,2006.
9. Niedermeyer,” E ,Alpha rhythms as physiological and abnormal phenomena”, International Journal of Psychophysiology ,vol. 26 ,no. 1-3, pp. 31-49, 1997.
10. 10- Feshchenko, Vladimir A, Reinsel, Ruth A and Veselis, “Multiplicity of the α Rhythm in Normal Humans”, Journal of Clinical Neurophysiology, vol. 18 ,no. 4, pp. 44-331, 2001.
11. Pfurtscheller, G. Lopes and Da Silva ,” Event-related EEG/MEG synchronization and desynchronization: Basic principles”, Clinical Neurophysiology, vol. 110 ,no. 11, pp. 57-1842, 1999.
12. Aurlien, H, Gjerde, I.O, Aarseth, J.H, Eldøen, G, Karlsen, B, Skeidsvoll, H and Gilhus N.E ,”EEG background activity described by a large computerized database”, Clinical Neurophysiology, vol. 115 ,no. 3, pp. 73-665, 2004.
13. Maan M. Shaker , “EEG Waves Classifier using Wavelet Transform and Fourier Transform”, International Journal of Biomedical Sciences , vol. 1 ,no. 2, pp. 85-90,2007.
14. Amjed S. Al-Fahoum and Ausilah A. Al-Fraihat , “Methods of EEG Signal Features Extraction Using Linear Analysis in Frequency and Time-Frequency Domains”, ISRN Neuroscience, vol. 2014 , pp. 1-7,2014.
15. C. E. Mohan Kumar And S. V. Dharani Kumar, “Wavelet Based Feature Extraction Scheme of Electroencephalogram” international Journal of Innovative Research in Science, Engineering and Technology, vol. 3, no. 1, pp. 908-913, 2014

\* Corresponding author.